

# Impact of Skin Pigmentation on Pulse Oximetry SpO<sub>2</sub> and Wearable Pulse Rate Accuracy: A Meta-Analysis

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## Abstract

**Background:** Photoplethysmography (PPG) is a technology routinely used in clinical practice to assess blood oxygenation (SpO<sub>2</sub>) and pulse rate (PR). Skin pigmentation may influence accuracy, leading to health outcomes disparities.

**Objective:** This meta-analysis primarily aimed to evaluate the accuracy of PPG-derived SpO<sub>2</sub> and PR by skin pigmentation. Secondly, we aimed to evaluate statistical biases and the clinical relevance of PPG-derived SpO<sub>2</sub> and PR according to skin pigmentation.

**Methods:** We identified 23 pulse oximetry studies (N=59,684; 197,353 paired SpO<sub>2</sub>-arterial blood observations) and 4 wearable PR studies (N=176; 140,771 paired photoplethysmography-electrocardiography observations). We evaluated accuracy according to skin pigmentation group by comparing SpO<sub>2</sub> accuracy root-mean-square (Arms) values to the regulatory threshold of 3% and PR 95% limits of agreement (LoA) values to  $\pm 5$  bpm, according to the standards of the American National Standards Institute, Advancing Safety in Medical Technology, and the International Electrotechnical Commission. We evaluated biases and clinical relevance using mean bias and 95% confidence intervals (CI).

**Results:** For SpO<sub>2</sub>, Arms were 3.96%, 4.71%, and 4.15% and pooled mean biases were 0.70% (95% CI: 0.17 to 1.22), 0.27% (95% CI: -0.64 to 1.19), and 1.27% (95% CI: 0.58 to 1.95) for light, medium, and dark pigmentation, respectively. For PR, 95% LoAs were -16.02 to 13.54, -18.62 to 16.84, and -33.69 to 32.54 and pooled mean biases were -1.24 bpm (95% CI: -5.31-2.83), -0.89 bpm (95% CI: -3.70-1.93), and -0.57 bpm (95% CI: -9.44-8.29) for light, medium, and dark pigmentation, respectively.

**Conclusions:** SpO<sub>2</sub> and PR measurements may be inaccurate across all skin pigmentation groups, breaching FDA guidance and industry standards thresholds. Pulse oximeters significantly overestimate SpO<sub>2</sub> for both light and dark skin pigmentation, but this overestimation may not be clinically relevant. PRs obtained from wearables exhibit no statistically or clinically significant bias based on skin pigmentation.

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## Original Manuscript

## Original Paper

# Impact of Skin Pigmentation on Pulse Oximetry SpO<sub>2</sub> and Wearable Pulse Rate Accuracy: A Meta-Analysis

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**Methods:** We identified 23 pulse oximetry studies (N=59,684; 197,353 paired SpO<sub>2</sub>-arterial blood observations) and 4 wearable PR studies (N=176; 140,771 paired photoplethysmography-electrocardiography observations). We evaluated accuracy according to skin pigmentation group by comparing SpO<sub>2</sub> accuracy root-mean-square (A<sub>rms</sub>) values to the regulatory threshold of 3% and PR 95% limits of agreement (LoA) values to  $\pm 5$  bpm, according to the standards of the American National Standards Institute, Advancing Safety in Medical Technology, and the International Electrotechnical Commission. We evaluated biases and clinical relevance using mean bias and 95% confidence intervals (CI).

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**Conclusions:** SpO<sub>2</sub> and PR measurements may be inaccurate across all skin pigmentation groups, breaching FDA guidance and industry standards thresholds. Pulse oximeters significantly overestimate SpO<sub>2</sub> for both light and dark skin pigmentation, but this overestimation may not be clinically relevant. PRs obtained from wearables exhibit no statistically or clinically significant bias based on skin pigmentation.

**Keywords:** health disparities, skin pigmentation; pulse oximetry; photoplethysmography

## Introduction

Photoplethysmography (PPG) technology has been used in medicine since the 1970s to assess pulse rate (PR) and blood oxygenation (SpO<sub>2</sub>). The accuracy of PPG-based SpO<sub>2</sub> and PR are critical for medical practice, clinical decision making, and patient outcomes [1].

Technological advancements have led to rapid expansion of this technology into consumer devices [2]. This has enabled consumers to continuously and unobtrusively track health status, generating information that is becoming commonly used in healthcare settings and as source of research endpoints [3,4].

Darker skin pigmentation may influence PPG-based SpO<sub>2</sub> and PR readings [5-8]. Patients with darker skin pigmentation are more likely than Caucasians to have overestimated SpO<sub>2</sub> leading to lower hospital admission, higher occult hypoxemia, and delayed or no access to dexamethasone, therapeutic oxygen, and COVID-19 therapies resulting in increased hospital readmission, organ dysfunction, and mortality [9-16].

Starting in 2013, a series of United States Food and Drug Administration (FDA) guidances, safety communications, and most recently attorney general statements have called to address darker skin pigmentation bias in pulse oximeters [17], yet these guidances lacked standards for assessing skin tone [18]. Recent pulse oximeter research has rekindled interest in skin pigmentation disparities in photoplethysmography (PPG) sensor accuracy, leading to increased media and regulatory attention [19-22]. In November 2023, over 24 attorney generals wrote a letter calling on the FDA to take urgent action to address pulse oximeter skin pigmentation disparities [23,24].

More recent research has also highlighted the potential presence of these biases in research-grade and consumer wearable PPG-based wearable devices [4,25-27], leading to calls to address inequity, bias, and discrimination in wearable health technology and clinical practice algorithms [28,29].

Accuracy guidance for pulse oximeters and heart rate/PR devices has been delineated by regulatory bodies, industry, and medical standards. Overall accuracy of pulse oximeters can be assessed with accuracy root-mean-square ( $A_{rms}$ ), which combines mean bias and precision (standard deviation of bias) into a single metric [30]. FDA guidance has a threshold of  $A_{rms} \leq 3\%$  [17] for transmittance devices and a threshold of  $A_{rms} \leq 3.5\%$  [17] for ear clip and reflectance devices, while international thresholds are set at  $A_{rms} \leq 4\%$  [30]. For heart rate/PR devices, overall accuracy can be assessed with 95% limits of agreement (LoAs). The American National Standards Institute (ANSI), Advancing Safety in Medical Technology (AAMI), and International Electrotechnical Commission (IEC) have set the recommendation that electrocardiography (ECG) devices have mean bias of  $\pm 5$  bpm or  $MAPE \leq 10\%$ , whichever is greater [31,32]. Devices with accuracy measures breaching these accuracy thresholds can produce questionable results.

It is therefore critical to generate evidence to inform the design and calibration of these devices to reduce algorithmic bias and improve accuracy, so that PPG based technology can generalize to all segments of the population, mitigating racial disparities in health outcomes. There have been systematic reviews on PPG skin pigmentation bias in pulse oximeters limited to either consumer device PR [33] or pulse oximeter SpO<sub>2</sub> [34-36]. Only one meta-analysis focused on pulse oximetry for this topic is available [34], and an additional 7 studies have been published recently, providing an additional 50,980 subjects and 182,369 paired observations. Therefore, performing a comprehensive meta-analysis to examine PPG accuracy, potential bias, and clinical relevance for SpO<sub>2</sub> and PR by skin pigmentation is timely.

## Methods:

This meta-analysis provides open code and data (Materials–Open Code and Data in Multimedia Appendix 1).

## Search Strategy and Selection Criteria:

We followed the PRISMA guidelines [37] and developed a MEDLINE systematic-review search. Searches were performed between April 2022 and June 2023 and a final ad-hoc search was conducted in June 2023. No additional studies were included after this date.

We included studies that: 1) Investigated PPG-derived SpO<sub>2</sub> or PR test devices per definition [38]; 2) used arterial blood gas (SaO<sub>2</sub>) or ECG as the reference device; 3) reported mean bias and standard deviation (SD), standard error (SE), 95% Limits of Agreement (LoA), or 95% confidence intervals (CI) by race, ethnicity, or skin tone. Inclusion disagreements were resolved by consensus.

Exclusion criteria included 1) literature reviews, systematic reviews, commentary, and meta-analyses; 2) non-English manuscripts; 3) unretrievable full source texts; 4) remote photoplethysmography (rPPG); and 5) lack of SaO<sub>2</sub>/ECG as reference device. We chose to not exclude papers based on measurement hardware or underlying algorithms given that all measurement devices relied on contact-based PPG to measure the same endpoints of interest—SpO<sub>2</sub> and PR.

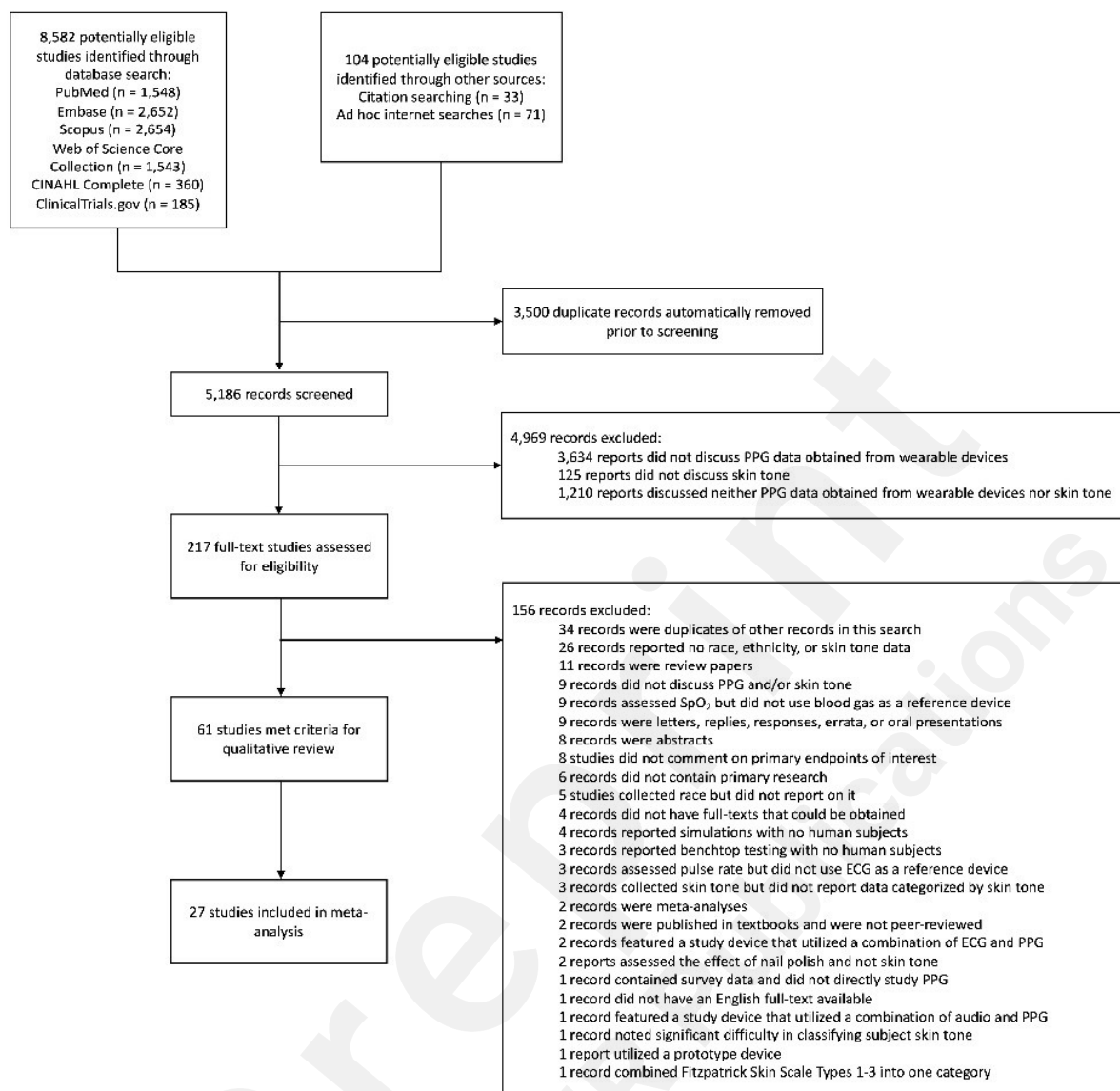
## Data Analysis

### Data Extraction

Data were independently extracted from published manuscripts (BWN and SS). A third and fourth reviewer (MB, HG) adjudicated any differences between the initial two reviewers and resolved any disagreements by checking manuscripts. First author verified the quality of manuscripts. Standardized data extraction was developed to extract the study characteristics (see Materials–Data Extraction in Multimedia Appendix 1). For one paper, we used participant-level data from supplementary materials to calculate mean bias and SE by skin pigmentation category [39]. This resulted in 27 studies in our final analysis (Figure 1, Table 1).

**Figure 1.** Study Selection Flow Chart.



**Table 1.** Characteristics of Included Studies.

Study (Author, Year)	Sample Size	Test Device Evaluated	Reference Device	SaO <sub>2</sub> (%) Range	Participant Population	Research Setting	Skin Pigmentation Method
<b>Pulse Oximetry</b>							
Abrams 2003 [41]	200	Nellcor N-200	Radiometer ABL-520	Not reported	Medical-patients Adult with cirrhosis	Inpatient	Race- Black and White
Adler 1998 [42]	298	Nellcor D-25	4-wavelength spectro-photometer, or co-oximeter (Radiometer	50 to 99	Medical-emergency patients	Inpatient	Skin Tone- Munsell color system categorized into light, medium, or dark

			OSM3)				
Andrist 2022 [43]	1,061	Not Reported	Not Reported	Not Reported	Medical-Pediatric	Inpatient	Race
Barker 2023 [44]	75	Masimo SET® pulse oximeters with RD-SET® sensors	Radiometer ABL-835 Flex CO-Oximeter	70 to 100	Mixed- Healthy and mild systemic disease	Research-Lab	Race
Bickler 2005 [8]	23	-Nellcor N-595 with Nellcor OxiMax A finger probe -Novamatrix 513s models (two types) -Nonin Onyx models (two types)	Radiometer OSM3	60 to 100	Healthy- non-smoking	Research-Lab	Ethnicity- light (Northern European) and dark (African American)
Bothma 1996 [45]	100	Simed S100e Nihon Kohden Ohmeda 3740	IL482 Co-oximeter System	87·8 to 99·2	Medical-critically ill adult patients	Inpatient	Skin Tone- EEL reflectance spectrophotometer. All participants had dark skin tone
Burnett 2022 [46]	46,253	Unspecified Nellcor and Masimo devices	GEMStat Premier 3000	Not Reported	Medical- patients receiving anesthesia	Inpatient	Race and Ethnicity
Crooks 2022 [47]	2,997	Not reported	Not reported	Not reported	Medical- COVID-19	Inpatient	Race
Ebmeier 2018 [48]	394	Marquette Rac-4A monitors with Masimo sensors and Philips IntelliVue MP70 monitors with Philips Adult Reusable SpO <sub>2</sub> sensors	Radiometer ABL 800 FLEX arterial blood gas analyser	Not reported	Medical- multiple conditions	Inpatient	Ethnicity
Fawzy 2022 [15]	1,216	Not reported	ABL825, ABL827, or ABL90 blood gas analyzers	Not reported	Medical- COVID-19	Inpatient	Race and Ethnicity
Feiner 2007 [6]	36	Nellcor N-595 (OxiMax A adhesive probe) Nellcor N-595 (a clip-type probe) Masimo Radical (clip probe)	Radiometer OSM3 multiwavelength oximeter	60 to 100	Healthy- non-smoking	Research-Lab	Ethnicity- light (Caucasian), intermediate (Hispanic, Indian, Filipino, Vietnamese), and dark (African American) categories

		Masimo Radical (adhesive disposable probe) Nonin 9700 (clip-type probe) Nonin 9700 (disposable adhesive probe)					
Foglia 2017 [49]	36	Nellcor Oximax (Covidien) Masimo Rainbow SET Radical 7	Siemens Rapidlab 1265	60 to 92	Medical- Infants with cyanotic congenital heart disease and oxygen saturation <90%	Inpatient	Skin Tone- Munsell Color System
Jubran 1990 [50]	54	Nellcor pulse oximeter with disposable or reusable probes Ohmeda-Biox3700 pulse oximeter with reusable probe	CO-oximetry	Not reported	Medical- Critically ill, ventilator-dependent patients	Inpatient	Race- Black and White
McGovern 1996 [51]	8	Ohmeda 3700	IL 482 Co-oximeter	Not reported	Medical- Adults with stable condition with severe COPD	Research-Lab	Race- All White
Muñoz 2008 [52]	846	Minolta Pulsox-7	IL 682 co-oximeter	Not reported	Medical- Adults under assessment for long-term home oxygen therapy	Outpatient	Race- All White
Pilcher 2020 [53]	400	Carescape B450 monitor with Nellcor probe GE Dash 3000 Masimo Radical 7 Masimo SET Quartz (unspecified) Masimo SET Quartz Q400 Nonin 2120 Nonin 2140 Nonin Avant (unspecified) Nonin Avant 4000 Nonin Avant 9700 Nonin Lifesense Medair Novamatrix Model 512 Ohmeda Biox 3700E with a GE TruSignal or Nellcor probe Philips Intellivue MP70 with a GE TruSignal Nellcor or Philips probe Welch Allyn with a Nellcor probe	Radiometer ABL800	72 to 100	Medical- Hospitalized adult patients	Inpatient and Outpatient	Skin Tone- Fitzpatrick Scale categorized into light, medium, dark

Ruppel [54]	2023	774	Not reported	Not reported	Not reported	Medical- cardiac catheterization	Inpatient	Race
Sudat [55]	2023	8,735	Not reported	Not reported	Not reported	Medical- multiple conditions	Inpatient	Race
Thrush [56]	1994	25	Critikon Dinamap Plus Model 8700 Critikon Oxyshuttle Ohmeda 3700 Catalyst Research MiniOx IV	IL482 co-oximeter	80 to 100	Healthy- non-smoking adults	Research-Lab	Race- All White
Valbuena [10]	2022	372	Not reported	Not reported, blood gas analysis	Not reported	Medical- Adult patients with respiratory failure or COVID-19	Inpatient	Race and Ethnicity- White, Black, Hispanic, and Asian
Vesoulis [57]	2021	294	Nellcor SpO <sub>2</sub> module with Neonatal-Adult MAX-N adhesive SpO <sub>2</sub> sensor (Covidien) (used with either Philips IntelliVue MP70 or MX800 monitors)	Radiometer ABL800 Flex	Not reported	Medical- Preterm infants at neonatal intensive care unit	Inpatient	Race- White and Black
Wiles [58]	2022	194	Nellcor reusable SpO <sub>2</sub> probes or Mindray disposable SpO <sub>2</sub> probes (GE Healthcare B1x5 M/P monitor)	RAPIDpoint 500 analyser (Siemens Healthcare GmbH)	Not reported	Medical- Adult patients with COVID-19 pneumonitis	Inpatient	Race- Asian, Black, White, and Other
Zeballos [7]	1991	33	Hewlett-Packard HP-47201A Ohmeda Biox IIA	IL282 co-oximeter	Not reported	Healthy- non-smoking volunteers	Research-Lab	Race- All Black
<b>Pulse Rate</b>								
Bent et al. (2020) [39]		53	Empatica E4 Apple Watch Fitbit Charge Garmin Vivosmart 3 Xiaomi Miband Biovotion	BittiumFaros 180, Bittium Inc.	NA	Healthy	Research-Lab	Skin Tone- Fitzpatrick Scale 1 (n = 7) 2 (n = 8) 3 (n = 10) 4 (n = 9) 5 (n = 9) 6 (n = 10)

		Everion					
Nelson et al. (2019) [59]	1	Apple Watch 3 Fitbit Charge 2	Vrije Universiteit Ambulatory Monitoring System	NA	Healthy	Research- Real World	Skin Tone- Fitzpatrick Scale 1 (n = 1)
Sanudo 2019 [60]	45	Apple Watch (version not reported)	Polar Chest Strap	NA	Healthy	Research-Lab	Skin Tone- Fitzpatrick Scale 2 (n = 15) 3 (n = 15) 4 (n = 15)
Chow 2020 [61]	40	Garmin Vivosmart HR+ Xiaomi Mi Band 2	Polar H7 Chest Strap	NA	Healthy	Research-Lab	Ethnicity and Skin Tone- East Asian, Fitzpatrick Scale 3 and 4

## Quality assessment of the overall evidence

QUADAS-2 tool was used to evaluate risk of bias and applicability (Figure S1 in Multimedia Appendix 1). Funnel plots evaluated publication bias using the *metafor* package [40] (Figures S2 and S3 in Multimedia Appendix 1).

## Statistical Analysis

### Skin Tone Categorization

We mapped skin tone, race, and/or ethnicity into three primary skin pigmentation groups of light, medium, and dark, following published methodology [34], (see Table S7 in Multimedia Appendix 1) and examined biases for SpO<sub>2</sub> and PR by each skin pigmentation group (described below).

We elected to utilize this same skin pigmentation categorization schema as has previously been used with the goal of expanding upon the analysis of Shi et al. [34].

### Statistical Analysis Methods

The objective of the study was to assess whether the devices were accurate in estimating SpO<sub>2</sub> and PR when compared with a SaO<sub>2</sub> and ECG reference device, respectively, for each skin pigmentation group. If these measures were found to be inaccurate, biases were quantified and their clinical relevance was assessed. The analytical approach to execute these research objectives was formulated based on methodologies employed in prior meta-analyses within the discipline [34].

### Evaluation endpoints and criteria

A summary of the evaluation criteria employed can be found in Table 2.

**Accuracy:** To evaluate accuracy of SpO<sub>2</sub>, root mean square ( $A_{rms}$ ) was used as an additional measure of accuracy for SpO<sub>2</sub> because of its commonality in the regulatory space [17]. It was calculated as  $\sqrt{bias^2 + precision^2}$ , where precision is the standard deviation of bias [41,42].  $A_{rms}$  is useful in clinical settings because it provides a single metric that accounts for both the systematic error (bias) and the random error (precision) in measurements and it provides a comprehensive assessment of how close the measurements are to the true values. A lower  $A_{rms}$  value indicates better accuracy, meaning that the measurements are closer to the true values whereas a higher  $A_{rms}$  value suggests lower accuracy, indicating that the measurements are further away from the true values.

For SpO<sub>2</sub>, our study used the more strict  $A_{rms} > 3\%$  threshold to define inaccuracy as per FDA guidance [17]. We used this threshold as 22/23 (95.65%) of pulse oximeter studies used a transmittance device and only one used an ear clip, which would have set a more liberal threshold of 3.5%. To evaluate accuracy of PR, the 95% limits of agreement (LoA) of bias was used, and LoA was constructed as mean bias  $\pm$  1.96 \* standard deviation (SD). For PR, a pooled 95% LoA not bounded by  $\pm$  5 bpm was considered inaccurate per ANSI/AAMI/IEC standards [31,32].

**Bias:** To evaluate bias of both SpO<sub>2</sub> and PR, mean bias and its 95% CI were used. For each data point that compares the test with the reference device, bias was constructed as (test device - reference device). Based on the final results, a measure was considered to have statistically significant bias if the 95% CI of its mean bias did not contain 0, with the estimated mean bias over 0 indicating overestimation and under 0 indicating underestimation.

**Clinical relevance of Estimated Bias.** To evaluate the clinical relevance of the estimated bias for SpO<sub>2</sub>, if the 95% CI of mean bias was out of the  $\pm 4\%$  range it was considered clinically relevant. This threshold is inferred from FDA guidance on Pulse Oximeters - Premarket Notification Submissions [510(k)s]: Guidance for Industry and Food and Drug Administration Staff [17]. To evaluate the clinical relevance of the estimated bias for PR, if the 95% CI of mean bias was out of the bound of  $\pm 5$  bpm it was considered clinically relevant as per ANSI/AAMI/IEC standards [31,32].

**Table 2.** Evaluation Endpoints and Criteria.<sup>a</sup>

Category	Objective	Evaluation Endpoint	Evaluation Criteria
SpO <sub>2</sub>	Evaluate accuracy	A <sub>rms</sub>	Accurate if A <sub>rms</sub> $\leq 3\%$
	Statistically significant bias	Mean bias (95% CI)	Statistically significant bias if 95% CI does not contain 0
	Clinically relevant bias	Mean bias (95% CI)	Clinically relevant bias if either upper bound of 95% CI $< -4\%$ or lower bound of 95% CI $> 4\%$
Pulse Rate	Evaluate accuracy	95% LoA	Accurate if 95% LoA is bounded by $\pm 5$ bpm
	Statistically significant bias	Mean bias (95% CI)	Statistically significant bias if 95% CI does not contain 0
	Clinically relevant bias	Mean bias (95% CI)	Clinically relevant bias if either upper bound of 95% CI $< -5$ bpm or lower bound of 95% CI $> 5$ bpm

<sup>a</sup> A<sub>rms</sub> = accuracy root mean square, LoA = limits of agreement, CI = confidence interval.

### Statistical meta-analysis methods

To obtain pooled results for above listed endpoints, we collected sample size, paired observations, mean bias, and standard deviation from various studies. When not available, we either transformed relevant parameters, such as 95% LoA and 95% CI, into these statistics or obtained them by analyzing the raw data.

**Methods to pool measures of bias:** Correlated and hierarchical effects (CHE) models were used to pool mean biases from various studies. Specifically, three-level hierarchical models were constructed, with Level 1 representing individual data points collected in a study, Level 2 representing potentially multiple comparisons within a research study, and Level 3 representing various studies included in the meta-analysis. Within a study, there may be multiple devices being compared using the same participants data, and these effect sizes are dependent. To account for the dependence, the CHE model utilized robust variance estimation (RVE) method which allowed us to combine data from single-measure design studies with multiple dependent estimates of effect size, even when the dependence is unknown [62]. To execute the CHE model with RVE, we needed to plug in assumed correlation coefficients for these dependent effect sizes. We used correlation coefficient 0.9 following published methods [34], and small ( $\rho = 0.30$ ) and moderate ( $\rho = 0.60$ ) correlation coefficients were also explored in sensitivity analyses. Additionally, one report [47] had substantially larger SE and we conducted a separate analysis with their results removed as a part of the sensitivity analysis. To evaluate heterogeneity of the studies, we reported the overall  $I^2$  (percentage of variability in the effect sizes that is not caused by sampling error) and its breakdown of within-study ( $I^2_{Level2}$ ) and between-study ( $I^2_{Level3}$ ) portions. Forest plots were provided for visualization of mean bias (Figures S2 and S3 from Multimedia Appendix 1).

**Methods to pool measures of accuracy:** When it comes to providing pooled 95% LoA and A<sub>rms</sub>, no established methodologies exist, and we followed an analytical approach in prior meta-analyses within the discipline [34]. Specifically, SD of bias across studies were pooled using CHE models similar to those used to pool mean biases. And pooled mean bias and pooled SD were used to provide pooled estimates of 95% LoA and A<sub>rms</sub>. Specifically,

- Overall accuracy  $A_{rms} = \sqrt{\text{the pooled mean bias } s^2 + \text{the pooled } S D^2}$  ;
- Overall 95% LoA = pooled mean bias  $\pm 1.96 * \text{pooled SD}$ .

### Other methods

Descriptive statistics were provided for study characteristics, the device intended use, mean bias based on different skin tones, reference devices. All analyses were conducted using R (4.3.1). Statistical models were based on R packages *metafor* [40] and *clubSandwich* [63].

## Results

### Study Selection and Characteristics

Search strategy resulted in 8,582 records. We selected 27 studies for full review (pulse oximetry = 23, PR = 4; Figure 1, Table 1, Table 2). A total of 23 pulse oximetry studies involving 59,684 participants with 197,353 paired  $\text{SpO}_2$ - $\text{SaO}_2$  observations were included. Additionally, four PR studies with 176 participants and 140,771 paired PR-ECG observations were analyzed (Table 3).

**Table 3.** Summary Characteristics of Included Studies.<sup>b</sup>

Item	Sub Item	Pulse Oximetry N (Percent)	Pulse Rate N (Percent)
Participants/ participants		59,684	176
	Light	40,416 (67.72%)	31 (17.61%)
	Medium	9,967 (16.70%)	129 (73.30%)
	Dark	9,301 (15.58%)	16 (9.09%)
Paired Observations		197,353	140,771
	Light	131,008 (66.38%)	43,116 (30.60%)
	Medium	32,095 (16.26%)	90,733 (64.50%)
	Dark	34,250 (17.35%)	6,922 (4.92%)
Device Type Included in Study	Medical	23 (100%)	0 (0%)
	Non-Regulated	0 (0%)	4 (100%)*
Sensor Type	Transmittance	22 (95.65%)	0 (0%)
	Reflectance	1 (4.35%)	4 (100%)
Patient Population	Healthy	4 (17.39%)	3 (75%)
	Medical	18 (78.26%)	0 (0%)
	Healthy and Medical	1 (4.35%)	0 (0%)
	Not Reported	0 (0%)	1 (25%)
Research Setting	Medical Inpatient	15 (65.22%)	0 (0%)
	Medical Outpatient	1 (4.35%)	0 (0%)
	Medical Combined	1 (5.35%)	0 (0%)
	Research Lab	6 (26.09%)	3 (75%)
	Research Real World	0 (0%)	1 (25%)
Skin Pigmentation Method	Skin Tone	4 (17.39%)	4 (100%)
	Race	13 (56.52%)	0 (0%)
	Ethnicity	3 (13.04%)	0 (0%)
	Race and Ethnicity	3 (13.04%)	0 (0%)

<sup>b</sup> \* = Medical device defined as devices that received regulatory clearance for either  $\text{SpO}_2$  or PR.

## Descriptive Statistics on Race, Ethnicity, and Skin Tone

**Pulse Oximetry.** Skin pigmentation was classified by race in 13 (56.52%) studies, ethnicity in 3 (13.04%) studies, skin tone in 4 (17.39%) studies, and both race and ethnicity in 3 (13.04%) studies (Table 3). There were a total of 40,416 (67.72%) light skin pigmentation patients with 131,008 (66.38%) paired observations, 9,967 (16.70%) medium skin pigmentation patients with 32,095 (16.26%) paired observations, and 9,301 (15.58%) dark skin pigmentation patients with 34,250 (17.35%) paired observations.

**PR.** Skin pigmentation was classified by race or ethnicity in 0 (0.00%) studies, and skin tone in 4 (100%) studies (Table 3). There were a total of 31 (17.61%) light skin pigmentation participants with 43,116 (30.60%) paired observations, 129 (73.30%) medium skin pigmentation participants with 90,733 (64.50%) paired observations, and 16 (9.09%) dark skin pigmentation participants with 6,922 (4.92%) paired observations.

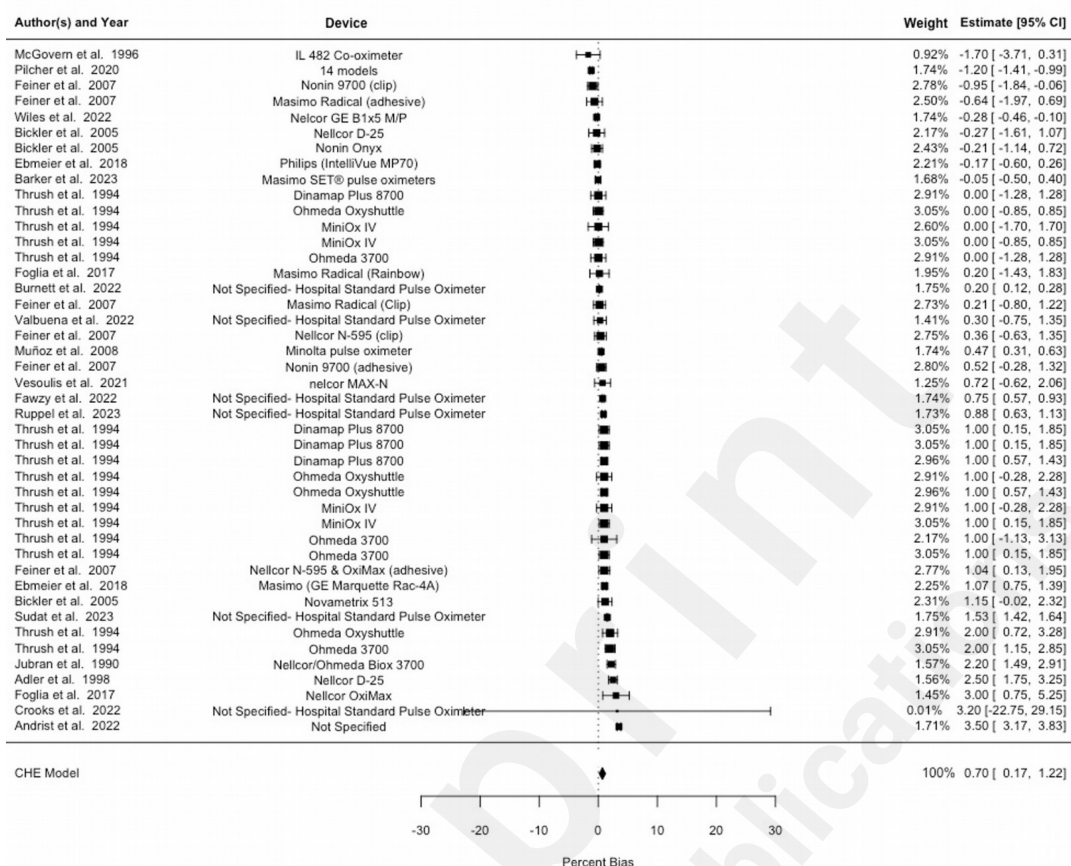
## PPG Accuracy and Bias by Skin Pigmentation

**Pulse Oximetry.** The pooled  $A_{rms}$  across different skin pigmentation groups was 3.6%, and 3.96%, 4.71%, and 4.15% for light, medium, and dark skin pigmentation, respectively (Table 4 and Figures 2-4). Of note, studies implementing multiple trial conditions or utilizing multiple study devices were shown multiple times in Figures 2-4 to delineate different devices used within the same study. We observed a pooled mean percent bias of 0.82% (95% CI: 0.29% to 1.35%) across all skin pigmentation groups using the CHE model. Between-study heterogeneity ( $I^2_{Level3}$ ) accounted for 14.53% of the total variation, while within-study heterogeneity ( $I^2_{Level2}$ ) explained 84.02% of total variation. Delineating by skin pigmentation, the pooled mean percent bias from the CHE model was 0.70% (95% CI: 0.17% to 1.22%) for light skin, 0.27% (95% CI: -0.64% to 1.19%) for medium skin, and 1.27% (95% CI: 0.58% to 1.95%) for dark skin. (Tables S1 and S3 in Multimedia Appendix 1).

**Figure 2.** Pulse oximetry forest plot for light skin pigmentation with multiple entries from the same study representing different devices examined [6, 8, 10, 15, 42-44, 46-58].

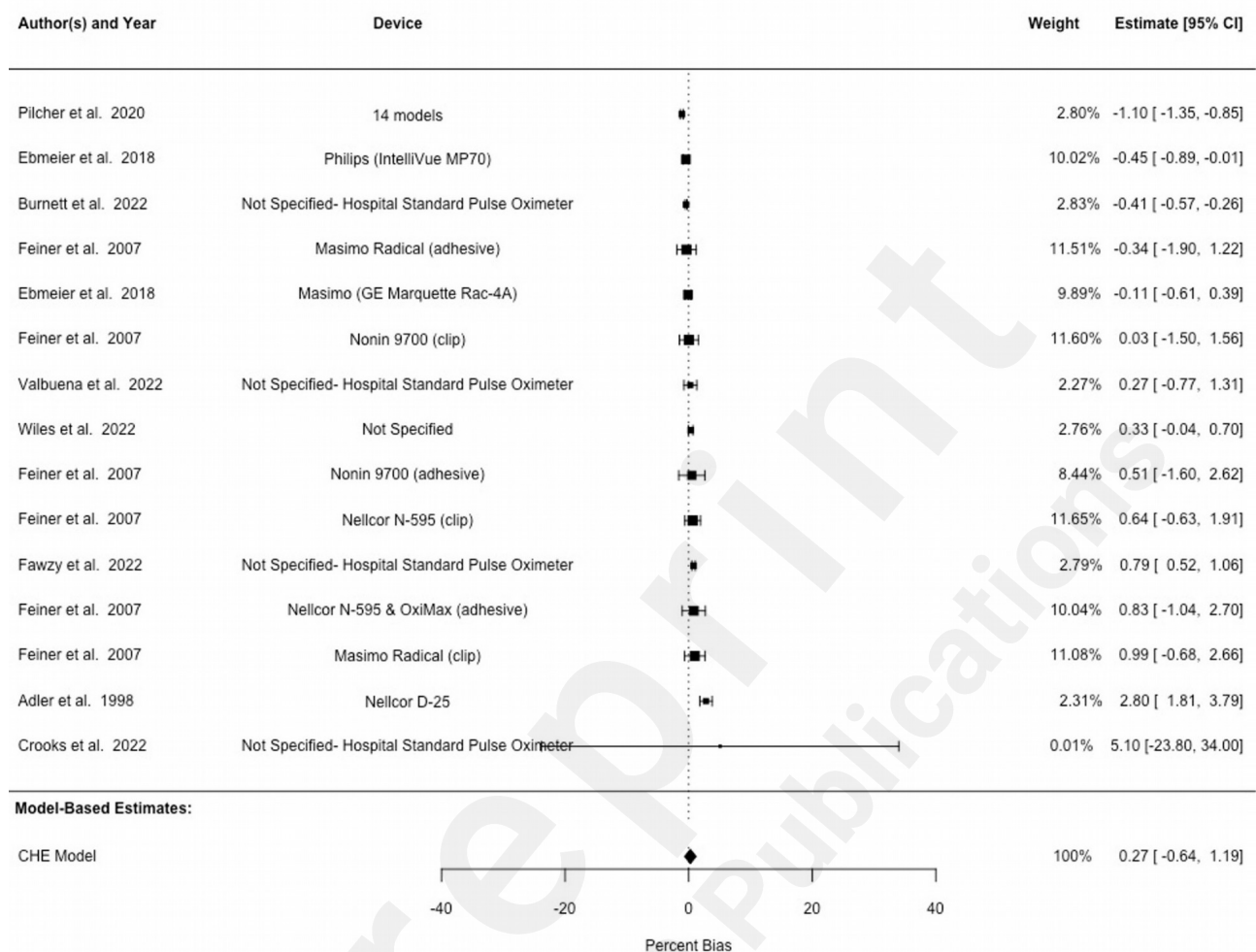


## Light Skin Tone Pulse Oximeter Bias

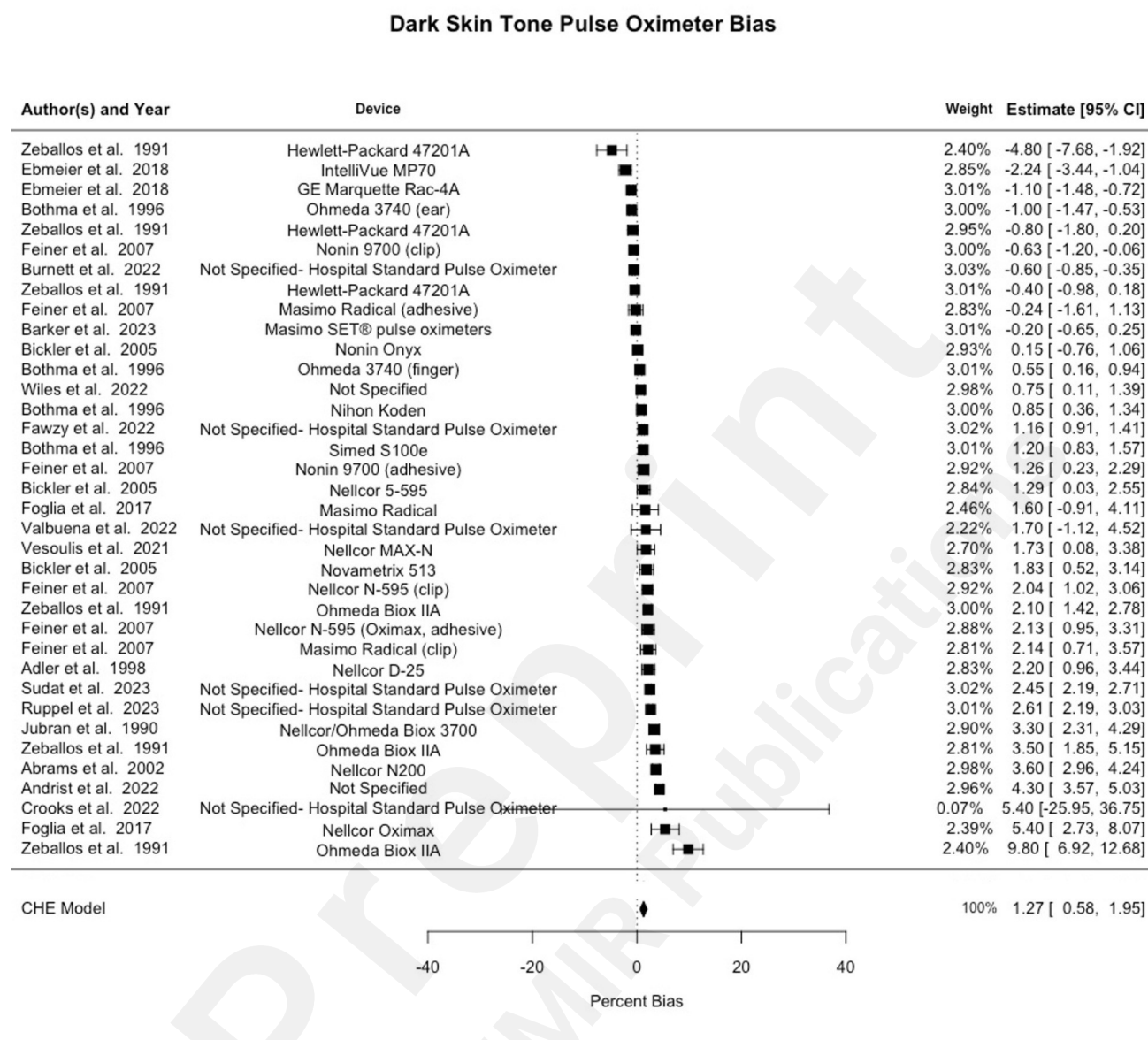


**Figure 3.** Pulse oximetry forest plot for medium skin pigmentation with multiple entries from the same study representing different devices examined [6, 10, 15, 42, 46-48, 53, 58].

### Medium Skin Tone Pulse Oximeter Bias



**Figure 4.** Pulse oximetry forest plot for dark skin pigmentation with multiple entries from the same study representing different devices examined [6-8, 10, 15, 41-50, 54, 55, 57, 58].



**Table 4.** Pulse Rate and Pulse Oximetry Bias by Skin Pigmentation.<sup>c</sup>

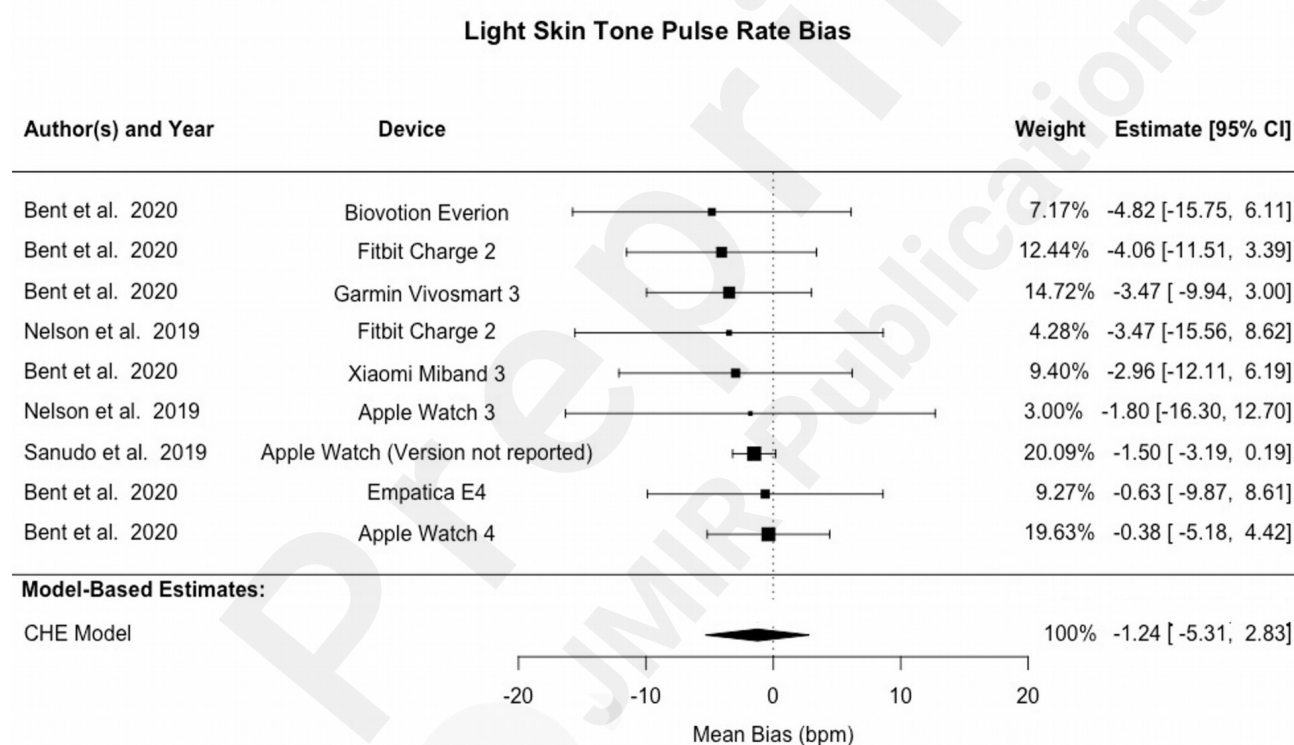
Table 1. Pulse Rate and Pulse Oximetry Bias by Skin Pigmentation										
Device Type	Skin Pigment. Category	Number of Studies (evaluations)	Sample size (data pairs)	Unit	Pooled Bias (95% CI)	Mean (SE)	Pooled SD (SE)	95% LoA	A <sub>rms</sub> %	Overall I <sup>2</sup> (between and within study heterogeneity)
Pulse Oximetry	Light	20 (44)	40,416 (131,008)	percent	<b>0.70 (0.17 to 1.22)</b>	3.90 (1.36)	-6.94 to 8.34	3.96**	97.45%	
	Medium	9 (15)	9,967 (32,095)	percent	0.27 (-0.64 to 1.19)	4.71 (1.71)	-8.95 to 9.50	4.71**	95.31%	
	Dark	19 (36)	9,301 (34,250)	percent	<b>1.27 (0.58 to 1.95)</b>	3.96 (1.30)	-6.49 to 9.02	4.15**	98.46%	
	Combined	23 (95)	59,684 (197,353)	percent	<b>0.82 (0.29 to 1.35)</b>	3.50 (1.28)	-6.04 to 7.68	3.60**	98.55%	
Pulse Rate	Light	3 (9)	31 (43,116)	bpm	-1.24 (2.83)	(-5.31 to 7.54 (2.13)	-16.02* 13.54*	to –	10.99%	
	Medium	3 (9)	129 (90,733)	bpm	-0.89 (1.93)	(-3.70 to 9.05 (1.75)	-18.62* 16.84*	to –	25.01%	

Dark	1 (6)	16 (6,922)	bpm	-0.57 8.29)	(-9.44 to 16.89 (1.31)	-33.69* 32.54*	to –	13.70% (NA and 13.70%)
Combined	4 (24)	176 (140,771)	bpm	-0.29 3.29)	(-3.87 to 8.64 (1.67)	-17.23* 16.65*	to –	30.66% (26.76%) and 3.90%)

<sup>c</sup>  $\rho = 0.9$  was used in CHE models to pool both mean bias and SD; Bold = statistically significant; \* = exceeds ANSI Standards for Pulse Rate; \*\* = exceeds FDA Guidance for Pulse Oximetry.  $A_{rms}$  = accuracy root mean square, LoA = limits of agreement, NA = not applicable as there was only one PR study with dark skin pigmentation. CI = confidence interval, SD = standard deviation, SE = standard error.

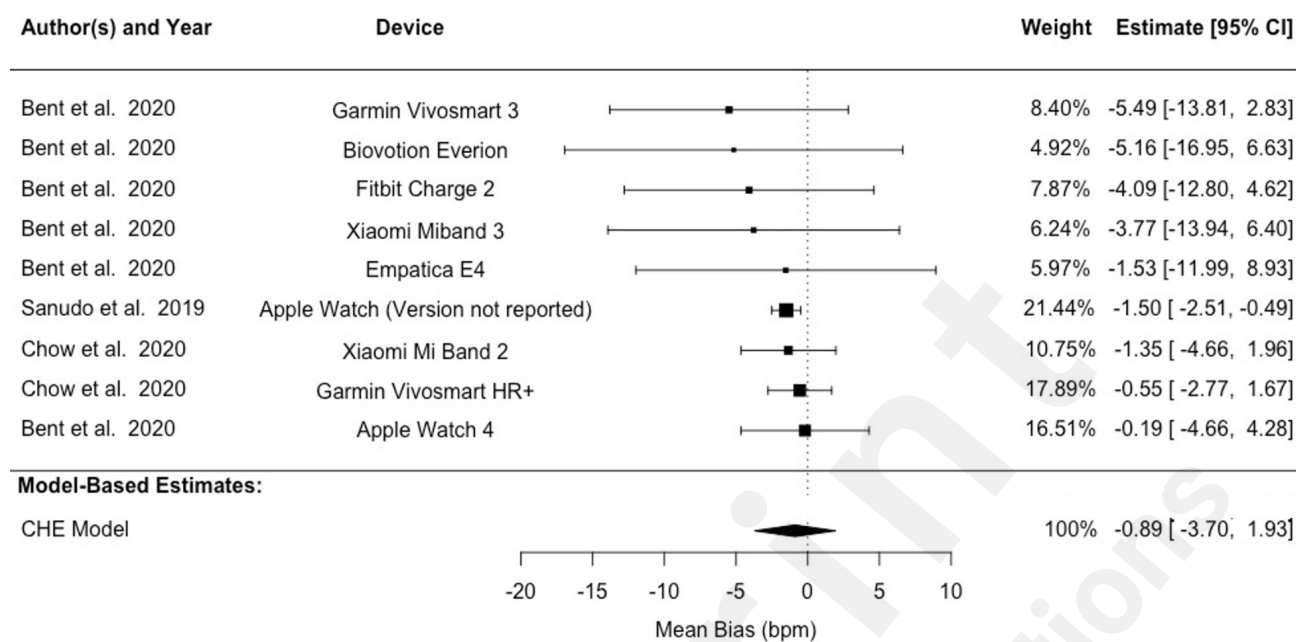
**PR.** Analysis using the CHE model revealed limits of agreement (LoA) of -17.23 to 16.65 bpm and a mean bias of -0.29 bpm (95% CI: -3.87 to 3.29 bpm) across all studies. Heterogeneity analysis demonstrated that 26.76% of the variation in bias ( $I^2_{Level3}$ ) stemmed from between-study differences, while 73.34% ( $I^2_{Level2}$ ) originated from within-study variation. Our analysis revealed 95% LoA of -16.02 to 13.54 bpm, -18.62 to 16.84 bpm, and -33.69 to 32.54 bpm for light, medium, and dark skin pigmentation groups, respectively. Mean biases were -1.24 bpm (95% CI: -5.31 to 2.83 bpm), -0.89 bpm (95% CI: -3.70 to 1.93 bpm), and -0.57 bpm (95% CI: -9.44 to 8.29 bpm) for the corresponding groups (Table 4 and Figures 5-7). Detailed results are provided in Tables S2 and S3 in Multimedia Appendix 1.

**Figure 5.** Pulse rate forest plot for light skin pigmentation [39, 59, 60].



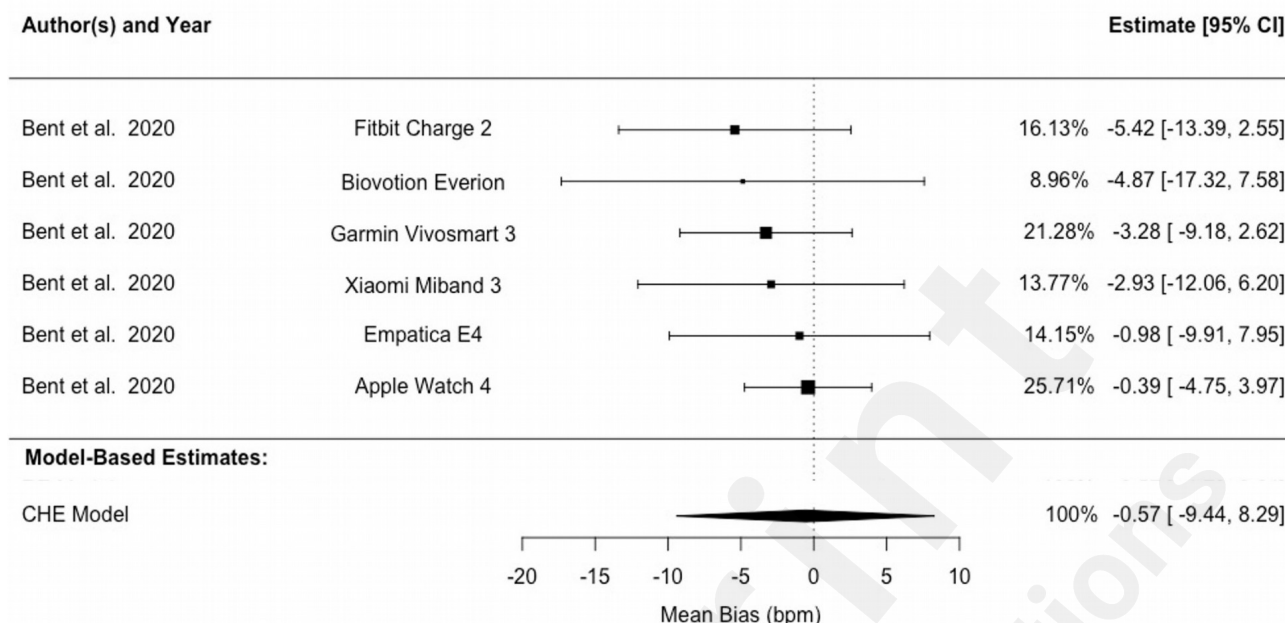
**Figure 6.** Pulse rate forest plot for medium skin pigmentation [39, 60, 61].

## Medium Skin Tone Pulse Rate Bias



**Figure 7.** Pulse rate forest plot for dark skin pigmentation [39].

### Dark Skin Tone Pulse Rate Bias



**Sensitivity Analyses.** Sensitivity analyses were performed for pulse oximetry SpO<sub>2</sub> by removing Crooks and colleagues [47] as an outlier due to substantially large SE (Tables S4 and S5 in Multimedia Appendix 1). The pooled mean percent biases and 95% LoA were essentially unchanged, while the pooled A<sub>rms</sub> across all skin pigmentation groups was 3.00%, 2.91%, and 3.40% for light, medium, and dark skin pigmentation, respectively. Sensitivity analyses using CHE models with a range of correlation coefficients (including small and moderate values) yielded similar conclusions to those obtained with a high correlation coefficient ( $\rho=0.9$ ), except for the PR analysis in the light skin pigmentation group. This analysis revealed a statistically significant bias when a low correlation coefficient ( $\rho=0.3$ ) was used. Details are provided in Table S4 in Multimedia Appendix 1.

## Discussion

The study revealed a paucity of studies properly assessing skin pigmentation and a tendency for uneven distribution across different skin pigmentation groups (overrepresentation of light skin for SpO<sub>2</sub> and a single study with representation of dark skin for PR), and lack of consumer-device reporting despite growing use in clinical setting. Results suggest inaccurate SpO<sub>2</sub> and PR measurements across all skin pigmentation groups as they breach FDA and ANSI/AAMI/IEC standards, respectively. Pulse oximeters may also overestimate SpO<sub>2</sub> significantly for light and dark skin pigmentation, but without clinically relevant bias. We did not find statistically significant or clinically relevant bias in wearable PR devices.

Despite not meeting FDA guidance across all groups, pulse oximeter SpO<sub>2</sub> was inaccurate only across medium and dark skin pigmentation groups when compared to the more liberal international thresholds. And, in the sensitivity analyses without the outlier study of Crooks and colleagues [47], all pooled A<sub>rms</sub> values dropped, resulting in inaccurate pulse oximeter SpO<sub>2</sub> only for dark skin pigmentation and no group exceeding international thresholds.

The results showing pulse oximeters significantly overestimating SpO<sub>2</sub> were expected for dark pigmentation and supported by findings on patient outcomes [9-13,15], but overestimated values for light pigmentation were unexpected. Two possible reasons come to mind. First, less melanin in lighter skin could distort the PPG signal [16]. Second, devices calibrated on individuals with medium

skin pigmentation (note that 48% of the US population is categorized as Fitzpatrick Skin Tone Scale (FSTS) III [64]) may lead to inaccurate readings for both lighter and darker skin pigmentation, since both may be suboptimally represented during algorithm training and testing.

Overall, these findings suggest that when pulse oximetry devices are deployed in their setting of intended use (i.e., uncontrolled settings, such real-world medical settings and home environments with diverse patient populations), the performance observed in analytical validation studies may not generalize.

## Strengths and Limitations

There were a few limitations, mostly from limitations inherent in prior studies, that should be noted. First, our skin pigmentation categorization approach has strengths, but also limitations. It was an effort to overcome the reporting heterogeneity, and the tendency in the published literature to conflate data collection on race, ethnicity, and skin tone. This is particularly problematic as skin tone is a physiological concept (determined by the melanin amount in the basal layer of the epidermis), while ethnicity and race are largely social constructs, with high underlying physiological heterogeneity [64]. To reduce heterogeneity, this meta-analysis reclassified race, ethnicity, and skin tone into a universal schema for skin pigmentation based on the system used by Shi and colleagues [34]. This method, however, classifies most Caucasians in the US as light, rather than medium-skin pigmentation [64]. Second, there were only four prior PR studies that collected participant skin tone that also reported on device accuracy and only one that had participants with dark pigmentation. Third, our study utilized stated FDA and ANSI/AAMI/IEC standards as set thresholds to gauge device performance. It is possible that guidelines and thresholds cited in our study may change in the future, potentially limiting the applicability of the conclusions drawn in this paper. Fourth, our study chose to group papers utilizing a variety of patient populations and testing methodologies with the goal of aggregating the largest pool of data possible on which to draw conclusions across multiple contexts; future studies should delineate the effect of these and other moderating variables on SpO<sub>2</sub> and PR. Lastly, there are moderators that we didn't examine, such as medical versus healthy populations, degree of blood oxygenation, transmittance versus reflectance sensors, PPG light wavelength, or activity versus rest.

## Evidence Generation Guidelines for Future Analytical Validation Studies

The 2013 FDA guidance may be insufficient to ensure accuracy in pulse oximeters across all skin pigmentation and settings of intended use [17]. But there are now multiple FDA guidances for digital health tools requiring fit-for-purpose evidence as well as growing concern/guidance on clinical research diversity [4,28,29,65-71]. The FDA currently categorizes consumer devices, as low-risk wellness products, exempting them from stringent regulatory oversight. However, as these devices are integrated into clinical decision-making and used as tools in clinical research [3,4], it becomes crucial to understand and communicate their advantages and limitations. Increased reliance on consumer devices increases the demand for accurate devices whose performance features and potential impact on health outcomes are known with transparency. To generate fit-for-purpose evidence applicable to diverse population, here we propose 5 recommendations based on FDA guidance and literature [4,28,29,65-71]:

**Recommendation 1:** It is vitally important for medical pulse oximetry devices as well as non-regulated research and consumer devices to incorporate the V3 framework [72] for sensor verification and analytical validation of derived SpO<sub>2</sub> and PR values for regulatory submission before these metrics can be responsibly deployed in medical, consumer, and research settings.

**Recommendation 2:** When possible, analytically validate devices in settings of intended use [72], rather than relying on controlled laboratory settings where digits may be warmed prior to testing to maximize accuracy, and confirm device accuracy in all subgroups (sex, race, skin pigmentation,

healthy vs medical populations).

**Recommendation 3:** Use objective measures of skin pigmentation, rather than relying on race and ethnicity as this will reduce heterogeneity in studies and allow for a more accurate understanding of how skin pigmentation impacts device performance.

**Recommendation 4:** Industry should set a priori set maximum allowable difference thresholds using FDA and ANSI guidelines, properly power each subgroup, and require that 95% LoA fit within these standards for each subgroup and in the setting of intended use before receiving regulatory approval, production, and deployment.

**Recommendation 5:** Future studies should report device and firmware versions as firmware updates may include changes in underlying algorithms influencing accuracy of metric generation as described previously in the literature [4].

## Conclusions

PPG has been applied in clinical practice for decades, and its accuracy in patients with different skin pigmentation has long been in question. Whether this technology contributes to diagnostic biases and by how much, is only more pressing for clinicians and patients with the advent of consumer wearable PPG sensors and the growing interest and incorporation of these devices into clinical practice and in clinical research. This meta-analysis found pulse oximeter SpO<sub>2</sub> and wearable PR were inaccurate across all skin pigmentation groups as the resulting accuracy values breached FDA Guidance and ANSI/AAMI/IEC Standard thresholds, respectively, although pulse oximeter SpO<sub>2</sub> was only found to be inaccurate for dark skin pigmentation in sensitivity analyses. In addition, despite not exceeding clinically relevant bias thresholds, pulse oximeters were found to significantly overestimate SpO<sub>2</sub> for light and dark skin pigmentation. No systematic or clinically relevant bias was found in estimation of PR. The recommendations in this paper can help advise patients, study participants, care providers, device manufacturers, application developers, researchers, and legislators on best practices going forward.

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Author contributions:

Study concept and design: HG, SS, BWN

Data collection: HG, SS, MB, BWN

Data analysis and interpretation: BWN (data analysis and interpretation), CC (statistical method determination, code review)

Draft writing and review: BWN (abstract, introduction, methods, results, discussion, review), GH (methods, discussion, review), SS (methods, review), SS (review), MB (methods), CC (methods, review).

All authors have had full access to all the data in the study, final responsibility for the decision to submit for publication, and had direct access and verification of the underlying data reported in the manuscript.

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## Conflicts of interest

BWN, MB, SS, and CC report employment and equity ownership in Verily Life Sciences.

## Abbreviations:

JMIR: Journal of Medical Internet Research



PPG: photoplethysmography

ECG: electrocardiography

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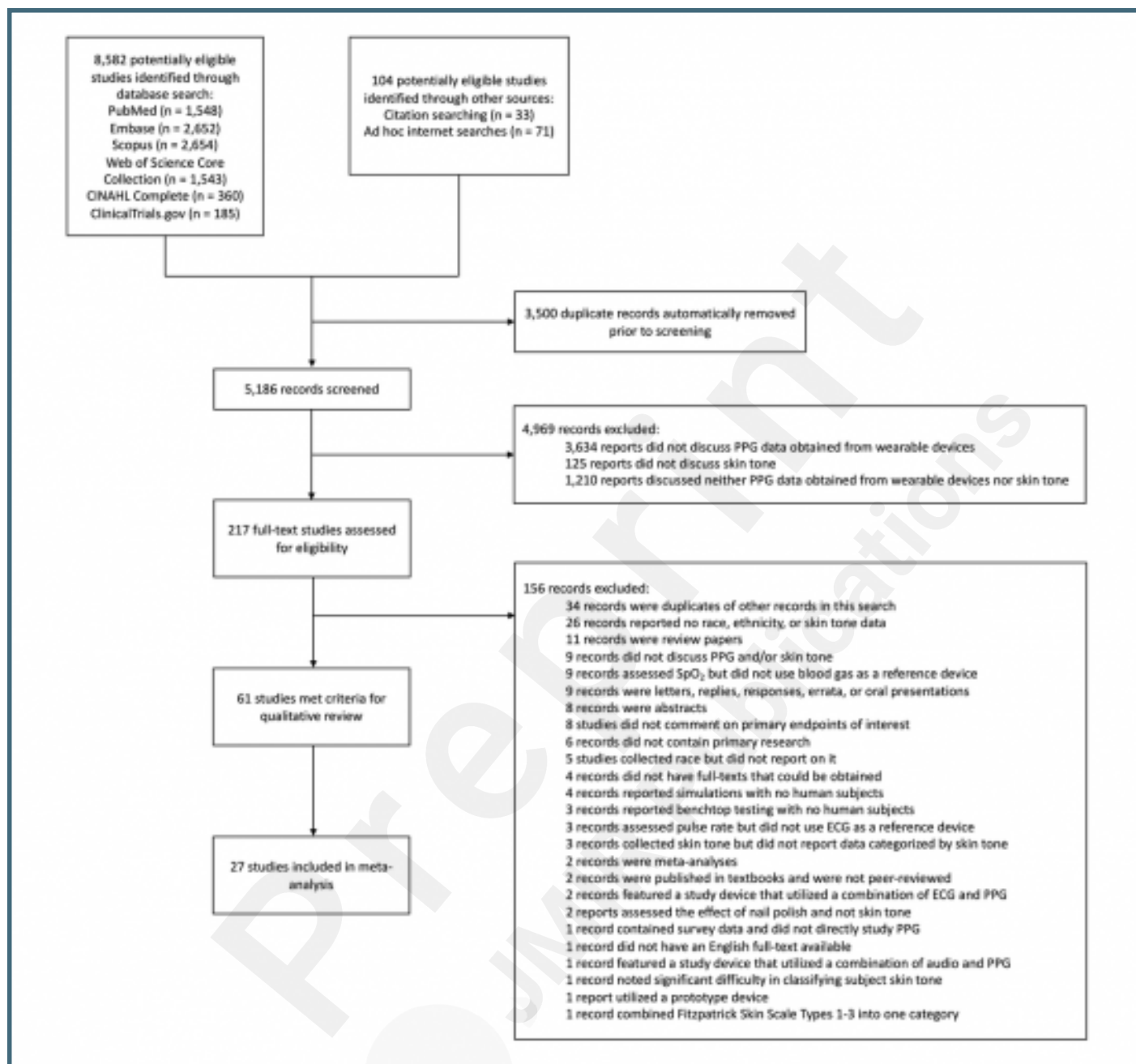
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## Supplementary Files

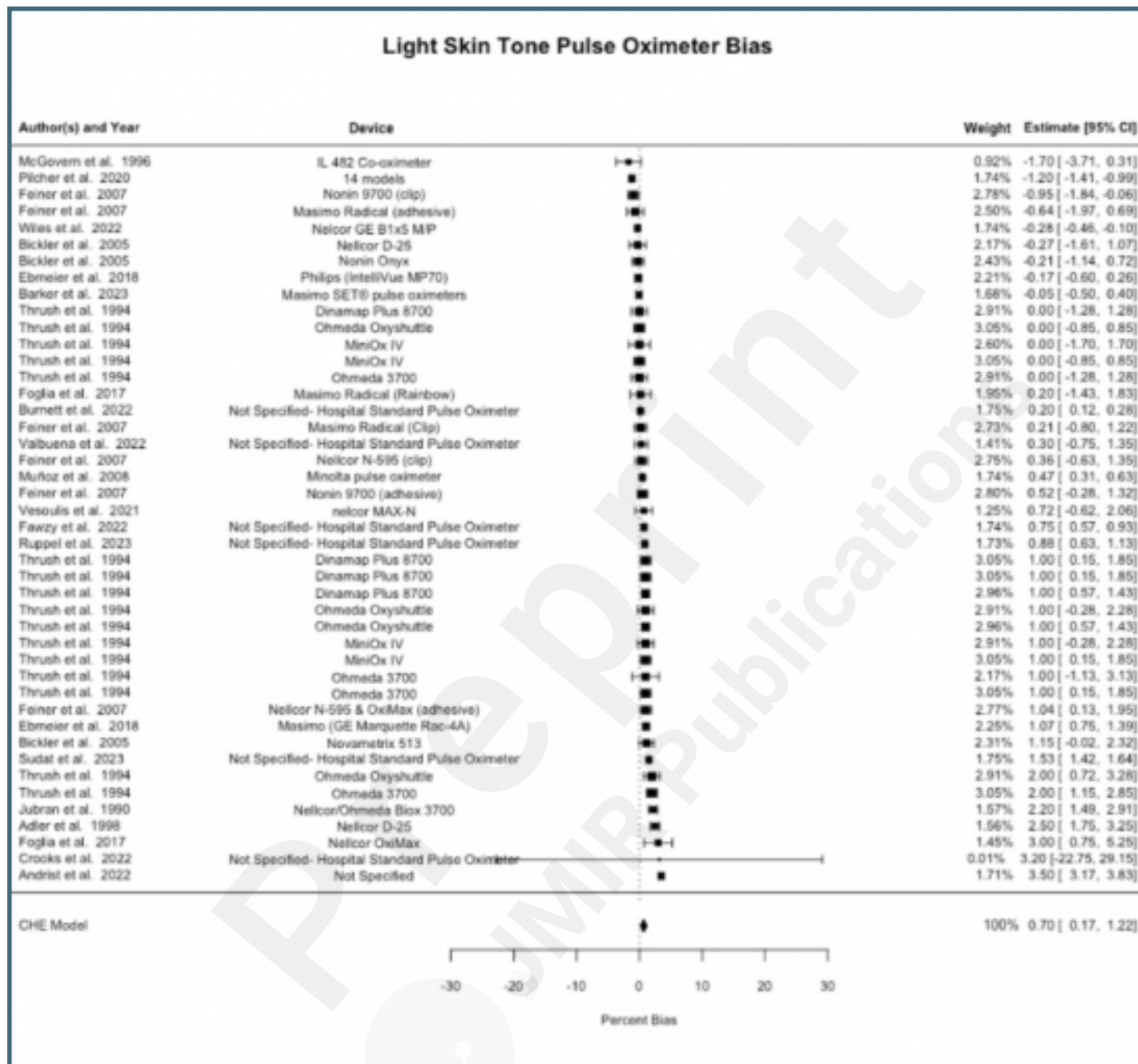
## Figures



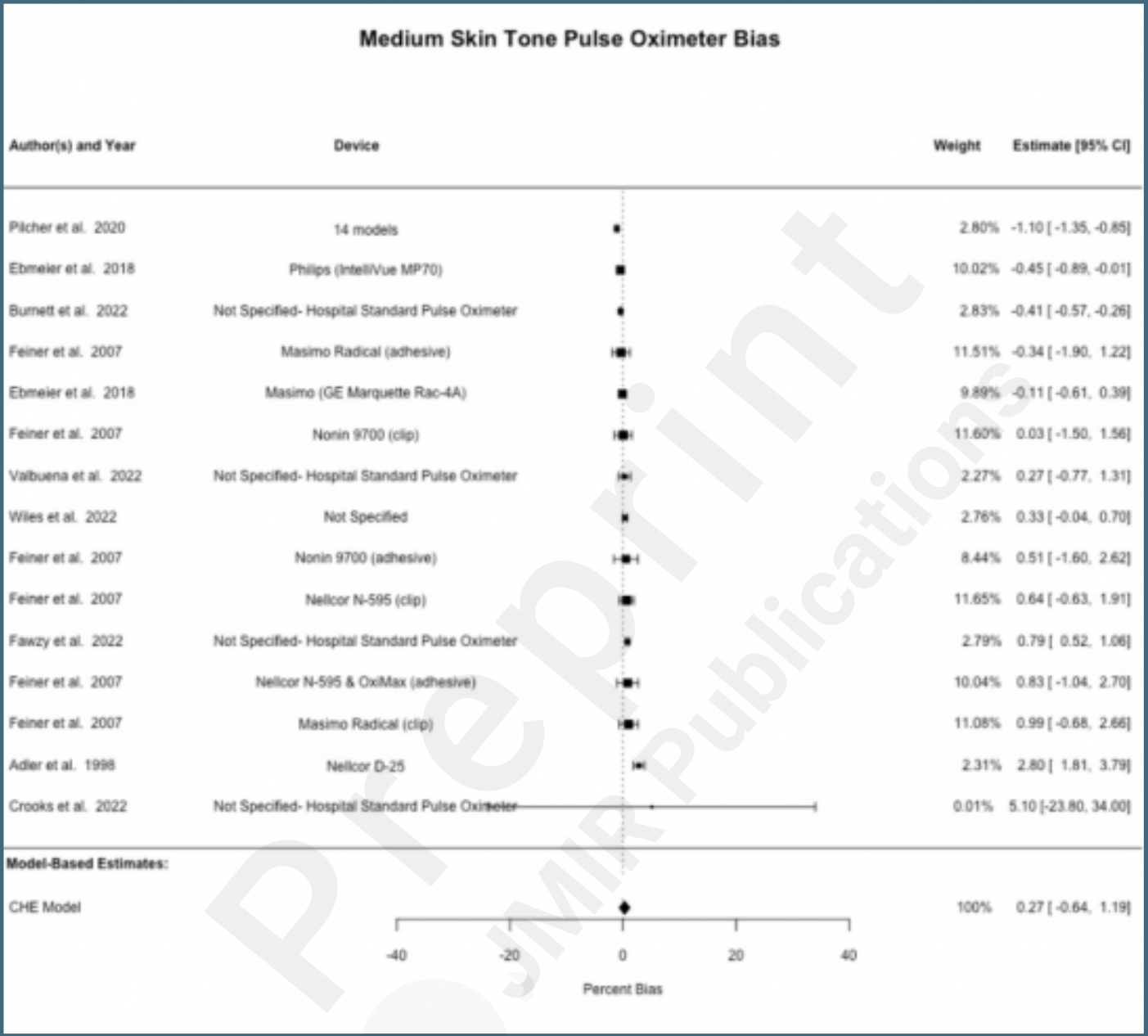
## Study selection flow chart.



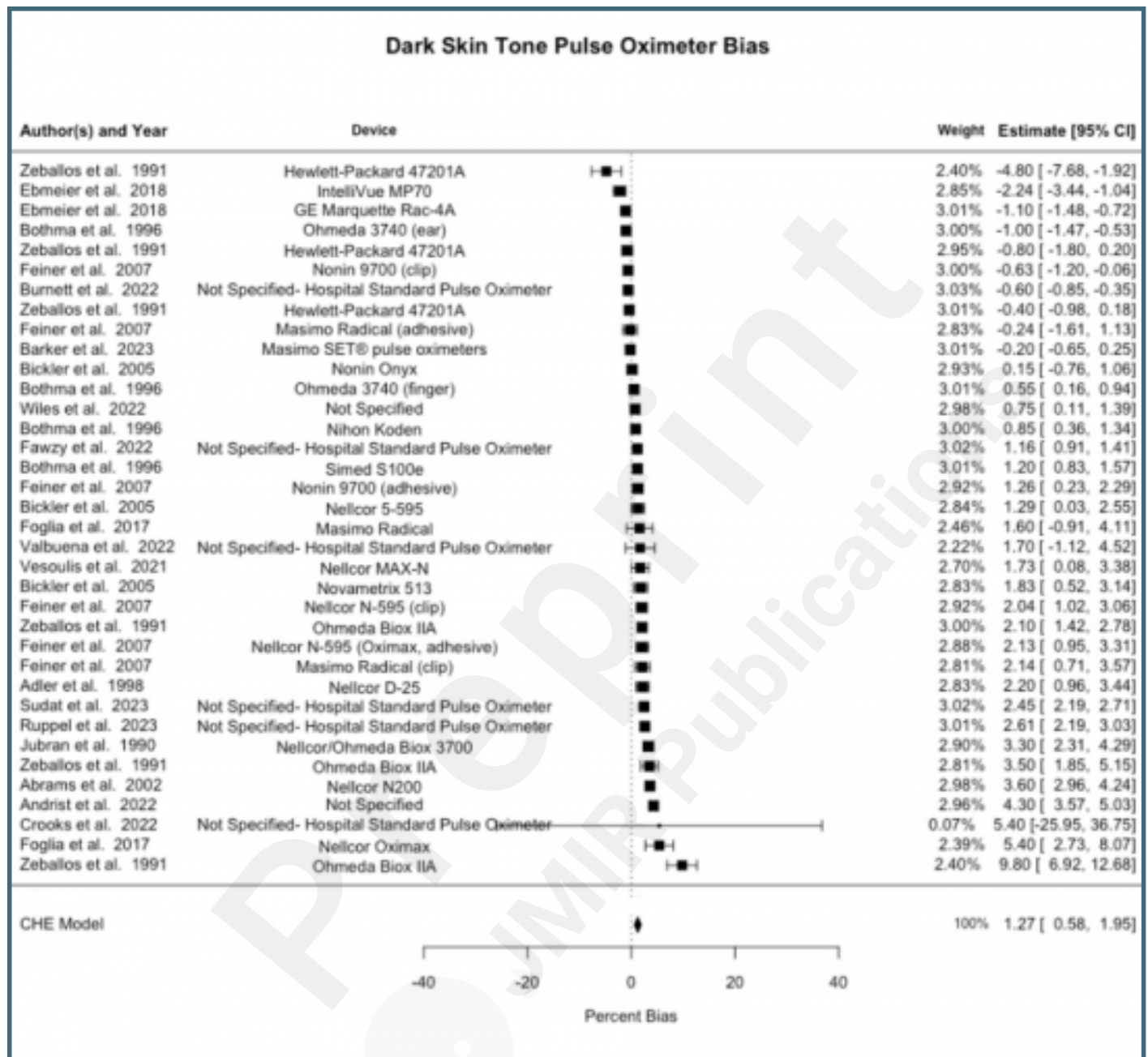
Pulse oximetry forest plot for light skin pigmentation with multiple entries from the same study representing different devices examined [6, 8, 10, 15, 42-44, 46-58].



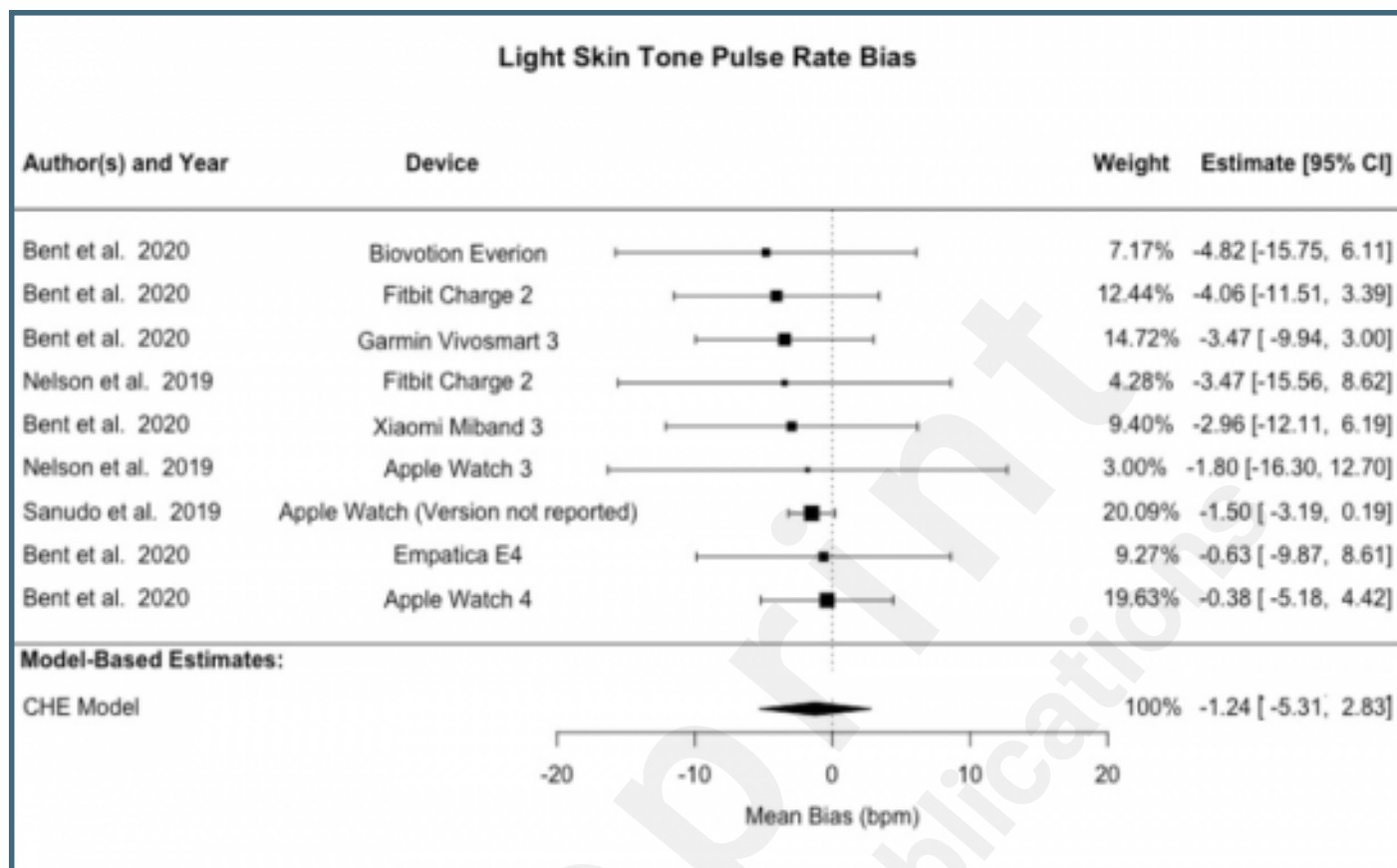
Pulse oximetry forest plot for medium skin pigmentation with multiple entries from the same study representing different devices examined [6, 10, 15, 42, 46-48, 53, 58].



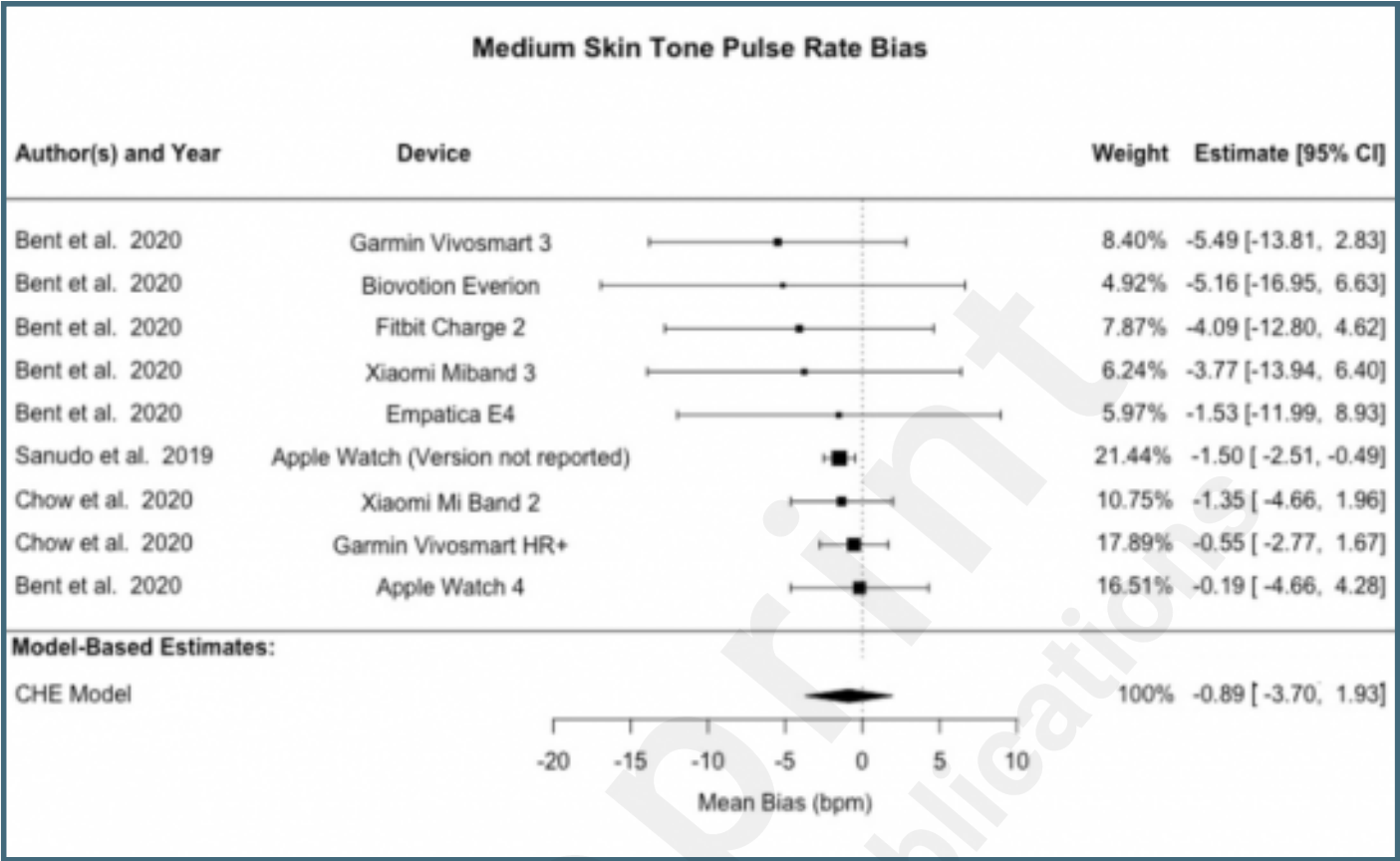
Pulse oximetry forest plot for dark skin pigmentation with multiple entries from the same study representing different devices examined [6-8, 10, 15, 41-50, 54, 55, 57, 58].



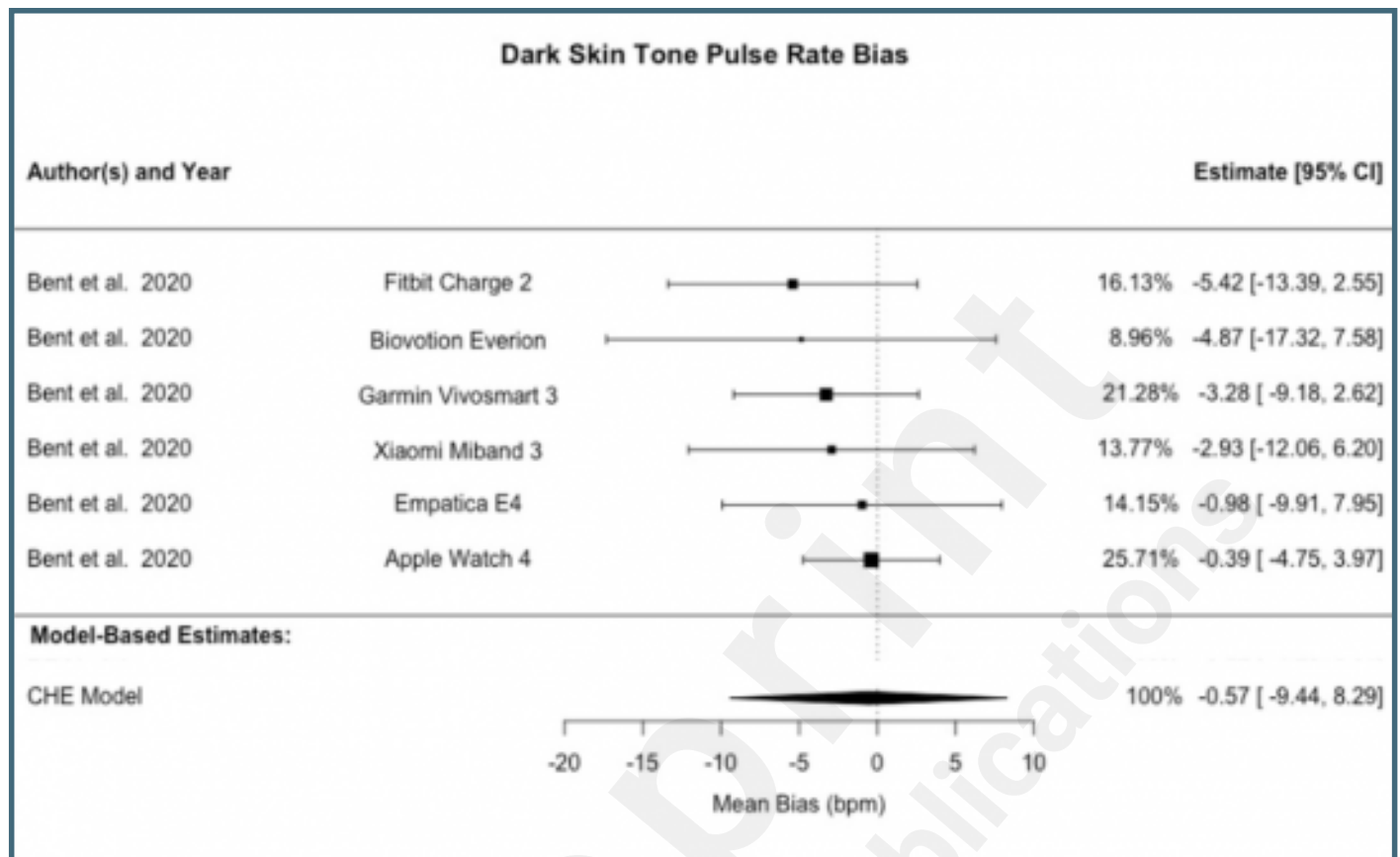
Pulse rate forest plot for light skin pigmentation [39, 59, 60].



Pulse rate forest plot for medium skin pigmentation [39, 60, 61].



Pulse rate forest plot for dark skin pigmentation [39].



## **Multimedia Appendixes**



Supplementary information.

URL: <http://asset.jmir.pub/assets/84686b6479e0d3adb5869174c731710c.docx>



## CONSORT (or other) checklists

PRISMA 2020 Checklist.

URL: <http://asset.jmir.pub/assets/55caa205656f9fd62ecc212b8ec483f9.pdf>